INTRODUCTION

Sensorineural hearing loss (SNHL) is one of the most common problems in the elderly [1]. A conventional hearing aid (HA) is considered as the first treatment for SNHL [2]. For patients with symmetric SNHL, bilateral HAs are recommended to achieve the acoustic benefits from binaural hearing [3]. However, persuading patients with symmetric SNHL to receive bilateral HAs remains a challenge because of cost and convenience issues.

Several studies have reported a correlation between auditory deprivation and amplification by HA. In adults with asymmetric SNHL, an improvement in suprathreshold speech recognition scores was observed for the affected ear by hearing amplification, which indicated resolution of the auditory deprivation [4]. In the studies that compared individuals with unilateral HA and those with bilateral HA, the interaural difference in the word recognition score (WRS) was relatively more preserved in the latter, indicating that HAs can prevent auditory deprivation [5,6]. The test for speech intelligibility generally involves evaluation of the optimum performance for phonetically balanced word recognition at the most comfortable listening level. This optimum performance is also known as the phonetically balanced maximum (PBmax) [7], which is determined by both peripheral and central auditory processing. Nevertheless, PBmax could be adjusted after HA use because a properly fitted HA increases...
the audibility of parts of the affected frequency range and, thus, enables more information to be presented for central auditory processing. In addition, HAs can stabilize speech intelligibility, as confirmed by the findings of previous studies that demonstrated a greater decrease in PBM for HA-unaided ears than for HA-aided ears [4,8]. However, conditions that aggravate auditory deprivation in patients with symmetric SNHL have not been deeply evaluated yet.

Meanwhile, digital signal processing enables complex processing beyond what is possible with analog aids with nonlinear processing, noise reduction, speech enhancement, and feedback reduction [9]. Additionally, the NAL-NL2 fitting program helps to achieve better speech intelligibility and overall loudness comfort [10]. However, we are unsure as to whether these advantages with the nonlinear and digital HAs actually affected auditory deprivation in the unilateral HA fitting condition or not.

Therefore, in the present study, we compared the changes in WRS between the HA-aided ear and the HA-unaided ear in patients with symmetric SNHL who received a unilateral digital signal processing and nonlinear HA. We also analyzed subgroups that were more susceptible to auditory deprivation after unilateral HA insertion.

**MATERIALS AND METHODS**

**Subjects**

Between 2001 and 2016, patients who received conventional HAs at the Department of Otorhinolaryngology in Severance Hospital, Seoul, Korea were retrospectively reviewed. We set our standard to recruit patients with strict criteria. First, we selected patients with symmetric SNHL (<10 dB difference) who were fitted with only a unilateral HA (ipsilateral ear), though the majority of patients with symmetric hearing loss had bilateral HA fittings. Second, we selected patients who used their HA for >1 year and 8 hours every day until the last visit. From these strict criteria for the enrollment, only 47 adults with symmetric SNHL who received a unilateral HA were retrospectively recruited for this study.

The included patients were aged 25–82 years (mean ± standard deviation [SD], 70.0 ± 13.8 years) and comprised 25 men and 22 women. The mean follow-up period was 31.0 ± 26.2 months (range, 12 to 108 months) from the date of HA insertion. All types of hearing loss in the participants were categorized as SNHL. All participants had used their HAs for >1 year with the acclimatization time of 2 months at least. Twelve patients received HA in the right ear, while the remaining received HA in the left ear. We prescribed and performed the computed tomography (CT) scan only if middle ear problems were suspected. CT showed the absence of pathological lesions in the middle ear or mastoid that could affect hearing conditions. All patients showed symmetric hearing loss, with air-bone gaps of <10 dB HL across all frequencies. Differences in the hearing threshold between the two ears were <10 dB HL. Following HA insertion, the change in the unaided hearing level was <5 dB HL (Table 1). We evaluated the average of aided pure tone thresholds at the very last session for each patient.

All patients used the digital, nonlinear type of HAs. The HA fitting program was NAL-NL2, which is the second-generation prescription procedure from The National Acoustic Laboratories for fitting wide dynamic range compression instruments. HA fitting for patients aimed at making good speech intelligible and overall loudness comfortable. We also fitted patients with real ear measurement to get more precise insertion gain. The types of HA used varied from an open-fit, receiver in the ear (RIC) type to a closed fit, complete in-ear type, depending on the patient’s preference and the condition of the external auditory canal. Proprietary signal processing techniques such as feedback cancellation and active noise cancellation were applied to all patients. In cases of RIC type, directional microphones were chosen. This study was approved by the local Ethics Committee of Yonsei University (No. 4-2017-0421). Since this is a retrospec-

**Table 1. Subject demographic data**

<table>
<thead>
<tr>
<th>Characteristics</th>
<th>Value (n=47)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Age at the fitting HA (yr)</td>
<td>70.0 ± 13.8</td>
</tr>
<tr>
<td>Sex</td>
<td></td>
</tr>
<tr>
<td>Male</td>
<td>25 (53.1)</td>
</tr>
<tr>
<td>Female</td>
<td>22 (46.8)</td>
</tr>
<tr>
<td>Side of wearing HA</td>
<td></td>
</tr>
<tr>
<td>Right</td>
<td>33 (70.2)</td>
</tr>
<tr>
<td>Left</td>
<td>14 (29.8)</td>
</tr>
<tr>
<td>PTA in HA-fitted ear (dB HL)</td>
<td></td>
</tr>
<tr>
<td>Initial PTA</td>
<td>53.6 ± 12.4</td>
</tr>
<tr>
<td>Last PTA</td>
<td>55.8 ± 11.5</td>
</tr>
<tr>
<td>PTA in unaided ear (dB HL)</td>
<td></td>
</tr>
<tr>
<td>Initial PTA</td>
<td>49.4 ± 13.9</td>
</tr>
<tr>
<td>Last PTA</td>
<td>53.0 ± 13.2</td>
</tr>
<tr>
<td>Average of aided PTA (dB HL)</td>
<td></td>
</tr>
<tr>
<td>HA-fitted ear</td>
<td>44.4 ± 8.4</td>
</tr>
</tbody>
</table>

Values are presented as mean ± standard deviation or number (%).

HA: hearing aid; PTA: pure tone average of four frequency thresholds (0.5, 1, 2, and 4 kHz).
Audiological analysis

Audiological evaluations, including pure-tone audiometry and speech audiometry, were performed before and more than 1 year after HA insertion for the HA-aided and HA-unaided ears. The most recent data obtained for each patient were used for statistical analyses. The pure-tone air (250–4,000 Hz) and bone conduction (250–4,000 Hz) thresholds were measured using clinical audiometers in a double-walled audio booth. The mean pure-tone audiometry thresholds for air conduction at 0.5, 1, 2, and 4 kHz \( \text{PTA}_4 = \frac{(\text{threshold at } 0.5 \text{ kHz}+1 \text{ kHz}+2 \text{ kHz}+4 \text{ kHz})}{4} \) were calculated.

The speech recognition threshold was defined as the level at which patients heard and correctly repeated spondaic words 50% of the time. A spondee has two Korean syllables, with equal stress placed on each syllable. A word recognition test was performed to obtain the maximal WRS, which were measured at the most comfortable hearing level using 50 monosyllabic Korean words that are heard during everyday life. The Korean words were from a validated and standardized resource [11] and were phonetically balanced.

Statistical analysis

All statistical analyses were performed using IBM SPSS ver. 21.0 (IBM Corp., Armonk, NY, USA). The results of multiple experiments are presented as mean ± SD. Continuous variables were compared using Mann-Whitney test and Wilcoxon signed-rank test for evaluating differences between unpaired and paired groups, respectively. Multiple regression analysis was performed with stepwise selection using a general linear model. For all statistical tests, a \( P \)-value < 0.05 was considered to be statistically significant.

RESULTS

Comparison of the hearing threshold and WRS between HA-aided and HA-unaided ears

The initial PTA\(_4\) (before HA insertion) was 53.6 ± 12.4 dB HL.
for the ipsilateral ears and 49.4±13.9 dB HL for the contralateral ears; this indicated symmetric hearing thresholds in both ears (Fig. 1A). Even in the last pure-tone analysis after HA insertion, the symmetric thresholds obtained in pure-tone audiograms did not change (Fig. 1B). The most recently derived PTAs was 55.8±11.5 dB for the ipsilateral ear and 53.0±13.2 dB in the contralateral ear. Thresholds did not deteriorate by more than 5 dB when compared with the initial hearing thresholds on each side.

The most recent HA-aided PTA for the ipsilateral ear was 44.4±8.4 dB (Fig. 1B). Specifically, the hearing gains at 1,000 and 2,000 Hz were approximately 20 dB HL, indicating that HA insertion was reasonable. Subsequently, we analyzed changes in WRS (ΔWRS) in both ears. WRS decreased by 5.1%±12.5% in the ipsilateral ears 7.6%±16.5% in the contralateral ears; the difference between ears was statistically significant (P<0.05) (Fig. 1C). When we compared WRS in HA-aided ipsilateral ear and unaided contralateral ear, the difference in change of WRS was more significant between two ears (P<0.001) (Fig. 1D).

Effects of the initial hearing threshold on auditory deprivation in the HA-unaided ear
We also investigated whether the initial mean pure-tone audiometry thresholds affected the severity of auditory deprivation in the unaided ear. To compare patients with good and with poor initial hearing thresholds, we classified the patients according to PTAs ≥53 dB HL (poor hearing threshold) or <53 dB HL (good hearing threshold). The cutoff value of 53 dB HL was determined by analyzing receiver operating characteristic curve for predicting auditory deprivation with the best sensitivity and specificity, where auditory deprivation in unaided ear was defined as more than 5% of difference in ΔWRS between the HA-aided and HA-unaided ears. As a result, no significant difference in ΔWRS between HA-aided and unaided ears was observed in the group with good initial hearing thresholds, whereas a marked decrease of ΔWRS was observed in the group with a poor initial hearing threshold (Fig. 2).

In addition, the initial threshold in PTAs was strongly correlated with the difference in ΔWRS between the ipsilateral and contralateral ears, which was denoted as auditory deprivation in Fig. 3A. Auditory deprivation increased as the initial hearing...
threshold at PTA, deteriorated. However, the duration of HA use was not significantly correlated with auditory deprivation in the contralateral ear though auditory deprivation tended to be more severe in the patients with longer use of HA (Fig. 3B).

DISCUSSION

In the present study, we identified auditory deprivation in the unaided ear in patients with symmetric SNHL wearing a unilateral HA. Notably, patients with a poor initial hearing threshold exhibited more severe auditory deprivation in the unaided ear. The concept of auditory deprivation has generally been accepted for a number of years. Several studies have reported auditory deprivation in the unaided ear of patients wearing a unilateral HA [5,8,12,13]. However, no study has reported the conditions that lead to increased susceptibility to severe auditory deprivation in patients with unilateral HAs. In addition, most previous studies have used analogue, linear type of HAs, rather than the more advanced digital, nonlinear type of HAs. It can be speculated that patients wearing unilateral HAs with more advanced auditory rehabilitation functions are likely to exhibit more severe auditory deprivation in the unaided ear.

In the present study, we analyzed the severity of auditory deprivation after unilateral insertion of nonlinear, digital HAs. The difference in ΔWRS between the HA-aided (ipsilateral) and HA-unaided (contralateral) ears was approximately 3% after 31.0 ± 26.2 months from the date of HA insertion. Hurley [14] described that the prevalence of auditory deprivation at the unaided ear would be 8% at 3 years post fitting and 26% at 5 years post fitting. Although the duration of HA use were quite variable in the present study, nonlinear, digital types of HAs does not seem to have more severe unaided ear effect compared to the nonlinear, analogue types of HAs at the least. The author [14] also suggested a cutoff value for predicting auditory deprivation in a study involving 77 unilaterally and 65 bilaterally fitted adults. Auditory deprivation was observed in the unilaterally fitted individuals, with a mean initial pure-tone average of 46 dB HL (3 frequency average based on 500, 1,000, and 2,000 Hz), but not in the unilaterally fitted group, with a mean initial pure-tone average of 35 dB HL [14]. In the present study, we also found that the group with PTA ≥ 53 dB HL showed the more deteriorated auditory deprivation; several reasons such as different definition of auditory deprivation and type of word recognition test between two studies may be attributable to the difference of cutoff value. Therefore, it could be concluded that the amount of hearing loss plays a major role in the severity of auditory deprivation in digital, non-linear HAs as well as analogue, linear HAs.

Basically, bilateral HA fitting has been recommended for patients with severe-to-profound symmetric SNHL [15,16]. Byrne et al. [15] suggested that mildly impaired listeners, those fitted unilaterally performed as well, on average, as those fitted bilaterally. However, Aided localization ability test results supported bilateral fitting for moderately and severely hearing-impaired listeners [16]. Even in the studies with children with severe SNHL, bilateral HAs were reported to be mandatory to prevent auditory deprivation [12,17]. The other study showed that a bilateral HA benefit was predominantly observed with respect to speech reception in noise, listening effort, and localization. This effect tended to be larger for the severe hearing loss patients than for the mildly hearing-impaired subjects [18]. Further, Boymans et al. [19] suggested that the patients with more severe hearing loss showed a higher bilateral benefit for the speech recognition test than did patients with milder hearing losses. However, several issues, such as cost, convenience, and stigma, hinder the acceptance of bilateral HAs by individuals with symmetric SNHL. If such drawbacks of bilateral HA fitting were serious issues for patients with symmetric SNHL, unilateral HA fitting can be alternative choice for hearing rehabilitation in the limited cases who have good initial hearing thresholds (i.e. less than 53 dB). Nevertheless, we should enthusiastically encourage patients to get bilateral HAs because it becomes much more difficult to rehabilitate the auditory-deprived ear after unilateral HA fitting.

Meanwhile, WRS tends to be decreased even after wearing a HA in the aided ear. This may be associated with the feature of hearing loss over age. General aging of the auditory system seems to be the predominant factor. The relevant aging processes include damage to hair cells, loss of blood supply in the cochlea, and loss of nerve fibers in the central auditory system. Central auditory hearing loss results from both the general effects of biological aging and the effects of attenuation of neural input from ears that exhibit peripheral pathology [20]. This results the decreased speech understanding which is not improved by using HAs [21]. These may explain the cause of decreased WRS in the aided ear.

The present retrospective study has several limitations. This study reported patients’ WRS with live-voice materials. Although the speech test was performed by a skilled audiologist, their use of live-voice materials may have been insensitive to a difference between ears for PTA < 55 dB HL. In addition, relatively small size of samples could make a biased result that the duration of HA was not correlated with the severity of auditory deprivation, which was inconsistent with the previous studies. In the future study, case analysis with larger sample size is promising to get more concrete conclusions.

Unilateral HA fitting induces auditory deprivation in the unaided ear in patients with symmetric SNHL. Because auditory deprivation tends to occur easily in patients with severe-to-profound SNHL, bilateral HA insertion should be considered on the basis of the initial hearing function to prevent auditory deprivation in the unaided ear.

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CONFLICT OF INTEREST

No potential conflict of interest relevant to this article was reported.

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REFERENCES